

Cytotoxicity Studies of Superparamagnetic Iron Oxide Nanoparticles in Macrophage and Liver Cells

¹Aroonsri Priprem, ¹Pramote Mahakunakorn, ²Chunpen Thomas and ²Ian Thomas
¹Department of Pharmaceutical Technology, Faculty of Pharmaceutical Science,
²Department of Physics, Faculty of Science,
Khon Kaen University, Khon Kaen, 40002, Thailand

Abstract: Superparamagnetic Iron Oxide Nanoparticles (SPIONs) prepared by simplified co-precipitation were attractive as MRI contrast agents and drug carriers which could internally be manipulated under the influence of an external magnetic field and also cancer treatment due to additional hyperthermia effects. **Problem statement:** Macrophage and liver cells are potentially exposed to internal SPIONs, thus used for this cytotoxic tests for safety information of SPIONs. **Approach:** The SPIONs were physicochemically characterized by several instruments to ensure the production process. Cell viabilities, lipid peroxidation and nitric oxide produced after exposure to the SPIONs were conducted in normal macrophage and liver cells. **Results:** The approximately 15nm SPIONs produced had their structure confirmed by FTIR and X-ray diffraction and their magnetic properties probed by NMR. Macrophage and liver cells reacted differently to the SPIONs in dose- and time-dependent manners. Lipid peroxidation increased in macrophage cells, but not liver cells, after 24 h exposure to 100 $\mu\text{g mL}^{-1}$ of SPIONs, but decreased after 72 h. Pro-inflammatory effect on macrophage cells induced by the SPIONs and measured as nitric oxide was not observed. Concentration of SPIONs up to 25 $\mu\text{g mL}^{-1}$ did not alter cell function and morphology. **Conclusion:** SPIONs produced by our simplified co-precipitation are dose-dependent cytotoxic to macrophage and liver cells.

Key words: Cytotoxic, macrophage cells, liver cells, superparamagnetic iron oxide nanoparticles

INTRODUCTION

Nanoparticles of metal oxides often exhibit enhanced chemical, thermal, magnetic or biological properties which make them useful particularly in biomedical applications. Magnetic nanoparticles offer some attractive possibilities as they can be internally manipulated under the influence of an external magnetic field (Sun *et al.*, 2008; Shubayev *et al.*, 2009). Single-domain magnetic particles have generated growing interest since their introduction (Papell, 1965), due to their potential use in applications such as contrast agents, biosensors, seals, bearing dampers and lubricants and most recently they have demonstrated a new role in cognitive function in the human brain (Banaclocha *et al.*, 2010). Specialized applications of these magnetic particles impose strict requirements on their characteristics, such as chemical composition, size distribution and uniformity, crystal structure, stability of magnetic properties, surface structure, adsorption properties, solubility and low toxicity (Thorek *et al.*, 2006). Superparamagnetic Iron Oxide Nanoparticles (SPIONs) have been the most extensively investigated due to their excellent

biocompatibility and ease of synthesis for multifunctional biomedical applications such as cellular targeting and drug delivery, tissue repair, magnetic resonance imaging and magnetofection (Sun *et al.*, 2008; Shubayev *et al.*, 2009; Thorek *et al.*, 2006; Gupta and Gupta, 2005; Bhaskar *et al.*, 2010). Magnetic targeting particles and carriers have been granted multi-centre Phase I and II clinical trials for hepatocellular carcinomas (Pankhurst *et al.*, 2003). Biodistribution and intracellular delivery of magnetic nanoparticles to target cells is made possible by controlling particle size distribution, particle charge, surface chemistry, shape and microstructure (Sun *et al.*, 2008; Pankhurst *et al.*, 2003). SPIONs are commonly produced via chemical co-precipitation (Molday, 1984; Ma *et al.*, 2003), hydrothermal synthesis (Wang *et al.*, 2003; Xu and Teja, 2008), thermal decomposition (Pei *et al.*, 2007) and electro-precipitation (Marques *et al.*, 2008). Co-precipitation of ferrous (Fe^{2+}) and ferric (Fe^{3+}) ions by a base in an aqueous solution under anaerobic conditions is simple, reproducible and efficient. Co-precipitation in a non-aqueous system produces size-controlled mono-dispersed SPIONs (Sun and Zeng, 2002).

Corresponding Author: Aroonsri Priprem, Department of Pharmaceutical Technology, Faculty of Pharmaceutical Science, Khon Kaen University, Khon Kaen, 40002, Thailand

Typically, magnetic nanoparticles distribute to the liver (80-90%), spleen (5-8%) and bone marrow (1-2%). Their surfaces may interact with extracellular matrix components and the plasma cell membranes of macrophages, endothelial cells, skin epithelium, respiratory depending on the route of administration and particle size (Shubayev *et al.*, 2009). SPIONs are potentially capable to generate Reactive Oxygen Species (ROS) leading to oxidative stress which can be measured by lipid peroxidation. *In vitro* assays with cells usually employ cells which can model a response or phenomenon likely observed or sensitized by particles *in vivo* so as to reflect possible physiologic responses to the nanoparticles (Jones and Grainger, 2009). To monitor cytotoxicity of nanoparticles, phagocytic and hepatic cells are commonly used.

The cytotoxicity of SPIONs prepared by a co-precipitation method was investigated in macrophage and liver cells. Lipid peroxidation and nitric oxide, indicators of free radical and pro-inflammatory mediators, respectively, were monitored so as to identify effects of the SPIONs on cell functions.

MATERIALS AND METHODS

Chemicals: Iron (III) chloride (FeCl₃, Sigma, Germany), iron (II) chloride (FeCl₂·4H₂O, Sigma, USA), ammonium hydroxide (25% NH₄OH, Merck, Germany), polysorbate or Tween 80 (C₆₄H₁₂₄O₂₆, Sigma, USA), Dulbecco's Modified Eagle Medium (DMEM, Invitrogen, USA), dimethyl sulfoxide (DMSO, Sigma-Aldrich, Germany) and 3-(4, 5-dimethylthiazol-2-yl)-2,5-diphenyltetrazoliumbromide (MTT, Invitrogen, USA) were purchased and used as received. Greiss reagent was prepared from sulfanilamide (Sigma, USA) and N-1-naphthylethylenediamine dihydrochloride (Fluka, Germany).

Synthesis of Superparamagnetic Iron Oxide Nanoparticles (SPIONs): Co-precipitation occurred after heating (up to 160°C) a mixture of equal concentrations (in gram equivalent) of each of freshly prepared solutions of ferrous (Fe²⁺) and ferric (Fe³⁺) ions in deionized water, while thoroughly mixing using a homogenizer (Daihan Scientific, Seoul, Korea) and adjusting the pH to neutral by adding ammonium hydroxide. Black precipitates of SPIONs, retained through 3 layers of membrane filtration (pore size 0.2 μm), were cleaned with deionized water, absolute ethanol and hot air dried at 50°C.

Preparation of SPIONs for cell exposure: Dried SPIONs were suspended in 0.001% Tween 80 solution followed by sonication at 24 kHz (Hielscher

Ultrasonics UH50H, Germany) for 30 min, the final concentration being 1 mg mL⁻¹.

Characterization of SPIONs:

X-Ray powder Diffraction (XRD): Dried SPIONs were crystallographically investigated using an X-ray powder diffractometer (Philips PW 3710, Amelo, The Netherlands), at x-ray wavelength of 0.154 nm, 0.2° step of 2θ angle. An estimation of average crystallite size of the result was conducted based on Scherrer's line broadening equation, as follows:

$$D = \frac{k\lambda}{\beta \cos \theta} \quad (1)$$

Where:

D = The crystallite size

θ = The diffraction angle

λ = The x-ray wavelength (0.15406 nm being used in this study)

β = The full width at half maximum

K = An instrument constant, i.e., 0.89 in this study

Fourier Transform Infrared (FTIR) spectroscopy:

An FTIR spectrophotometer (Perkin Elmer Spectrum One FTIR spectrophotometer, Massachusetts, USA) was used to assay the SPIONs using a wave number range of 400-4000 cm⁻¹.

Nuclear Magnetic Resonance (NMR): NMR spin-relaxation time (T₂) of protons (¹H) was measured using an NMR relaxometer (Maran spectrometer, Resonance Instruments (now under Oxford Instruments), Surrey, UK) to monitor the magnetic properties of the nanoparticles in solution at 12.78 MHz and 25°C. The measurement used the Carr-Purcell Meiboom-Gill (CPMG) pulse sequence (Farrar and Becker, 1971) Care was taken to measure T₂ with minimal diffusion effects by using the half echo-time (TE/2) values as short as possible. The TE/2 values used were in the range of 40-500 μs with 100-4000 echoes. About 0.1 mL of each sample in a 6 mm diameter glass tube was used. Each T₂ data was averaged from triplicate samples which were homogeneously dispersed while measuring. The spin-spin relaxation rate due to the SPIONs (1/T₂^{*} or R₂^{*}) was estimated, by the following equation:

$$R_2^* = \frac{1}{T_2^*} = \frac{1}{(T_2)_{\text{sample}}} - \frac{1}{(T_2)_{\text{blank}}} \quad (2)$$

Morphology: The morphology of the product was observed by Transmission Electron Microscopy (TEM; Jeol JEM 2010, JEOL, Japan).

Cytotoxicity studies: Cell lines of Chang liver and macrophage, cultured in liquid Dulbecco's Modified Eagle's Medium (DMEM), were plated at a cell density of about 20,000 cells/well of the 24-well plates (Nunc, Denmark) or 96-well plates (Corning, USA) overnight in a 5% CO₂ incubator (Jencons PLS, RS Biotech, UK) at 37°C.

Cell viability using MTT (Jones and Grainger, 2009): The cultured cells were exposed to SPIONs at various concentrations and then incubated with MTT (0.5 mg mL⁻¹) for 30 min. The medium was removed and DMSO added to dissolve formazan crystals, the metabolite of MTT and, after thorough mixing, the optical density of each was recorded at 550-750 nm. Cell viability was calculated and expressed as percentage of the control (Wang *et al.*, 2009).

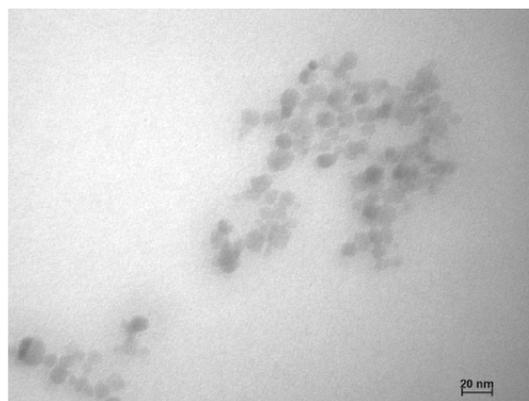
Lipid peroxidation by Malondialdehyde-Thiobarbituric Acid Reactive Substance (MDA-TBARS) assay: Malondialdehyde (MDA) content, a measure of lipid peroxidation, was assayed as Thiobarbituric Acid Reactive Substance (TBARS) (Ohkawa *et al.*, 1979). Thiobarbituric acid was added to the cultured medium, followed by perchloric acid. The mixture was incubated at 95°C for 15 min, cooled and centrifuged. The absorbance of the supernatant was measured at 550 nm and 550-750 nm using a microplate reader (BioRAD 680, Germany).

Measurement of Nitric Oxide (NO): NO production in cell culture medium was performed by employing Greiss reagent (1% sulfanilamide, 2.5% H₃PO₄, 0.1% N-1-naphthylethylenediamine dihydrochloride). The absorbance at 550 nm was measured and nitric oxide concentration was determined.

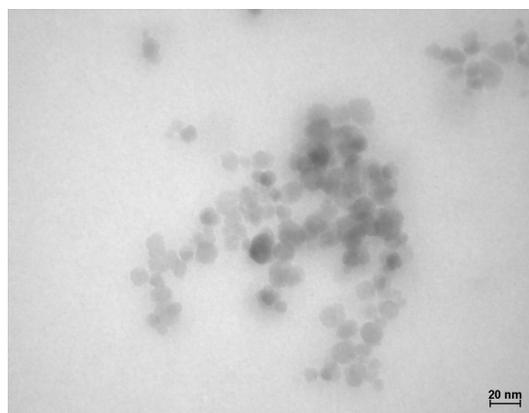
Statistical analysis: Quantitative analysis of the NMR relaxation time of the SPIONs was analyzed by linear regression analysis between concentration of the SPIONs and the 1/T₂. ANOVA was used to compare the results obtained from cytotoxicity.

RESULTS

TEM photographs of SPIONs, Fig. 1, demonstrate clusters of particles with a range of 5-15 nm in diameter. The clusters were formed by attractive forces between the dispersed magnetic nanoparticles in water. Those with and without polysorbate 80 gave an average size of 11.4±1.7 and 8.8±1.9 nm, as shown in Fig. 1a and b, respectively, suggesting that surfactant molecules did coat the surface of the SPIONs.



(a)



(b)

Fig. 1: Transmission Electron Microscope (TEM) photographs of the SPIONs (a) uncoated and (b) coated with polysorbate 80

An XRD pattern of SPIONs as shown in Fig. 2 demonstrates several peaks from 5-80°. There was no interference from the prominent peaks below 26° which resulted from the tape used to fix the SPIONs before mounting for analysis. These diffraction peaks at 30.3, 35.8, 43.4, 53.8, 57.3, 63.1 and 74.5° correspond to the respective crystal planes (220), (311), (400), (422), (511), (440) and (533) of a Fe₃O₄ crystal with a cubic spinel structure within error of ±0.5° (according to the PDF-890691, ICSD 082237 database). Calculation of average crystallite size using data from these peaks is based on Scherrer's line broadening equation (Wang *et al.*, 2007). The crystallite size of SPIONs produced was thus calculated as 14±3 nm, by Eq. 1.

The FTIR fingerprint of the SPIONs, Fig. 3, shows the strong absorption band at 580 cm⁻¹ of iron and oxide bonding for pure magnetites (Wang *et al.*, 2007), while the O-H band comes from water residue.

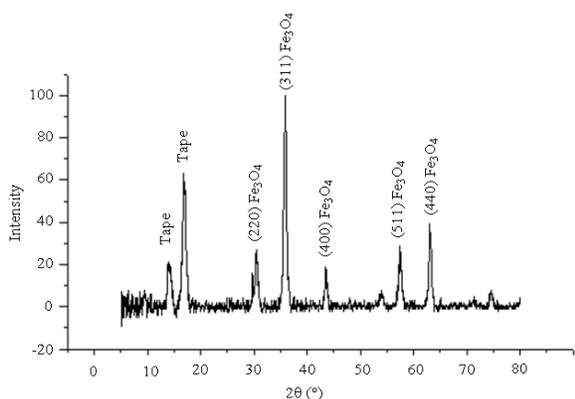


Fig. 2: XRD crystallographic pattern of SPIONs, fixed onto tape, at x-ray wavelength of 0.154 nm with 0.2° steps of 2θ

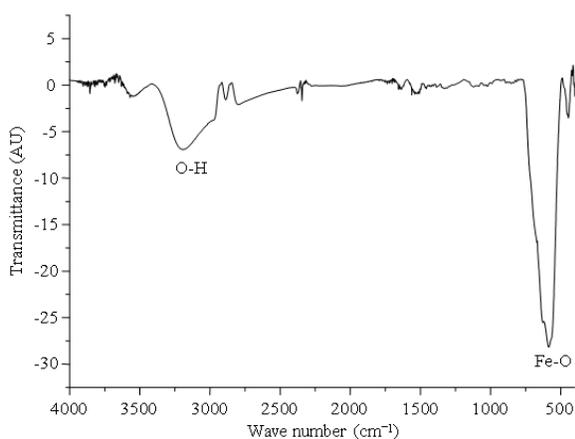


Fig. 3: FTIR graph of Fe₃O₄ magnetic nanoparticles synthesized by co-precipitation

Cytotoxicity study of SPIONs in macrophage and Chang liver cells: The purpose of this investigation was to evaluate potential toxicity and general mechanisms involved in SPIONs induced cytotoxicity, oxidative stress and pro-inflammatory response by MTT assay, TBARS assay and nitric oxide measurement investigated in an *in vitro* model derived from Chang liver cells or normal hepatocytes and macrophage cells. These cell lines have been well characterized for their relevance to toxicity studies and most concerns are about biodistribution of nanoparticles.

Cell viability after 24-h and 72-h exposure to SPIONs at 6.25, 12.5, 25, 50 and 100 μg mL⁻¹ to macrophage and normal hepatocytes suggested a potential dose dependence as shown in Fig. 4, but results were not significantly different (p>0.05).

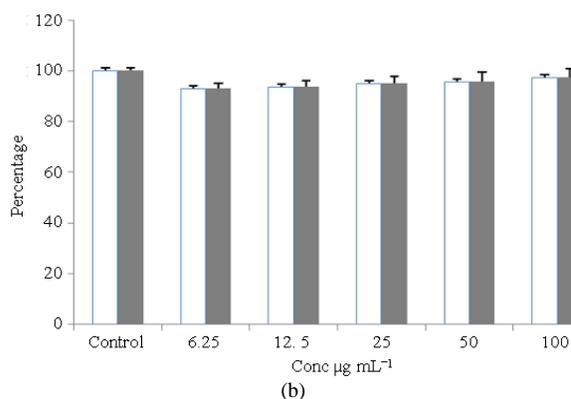
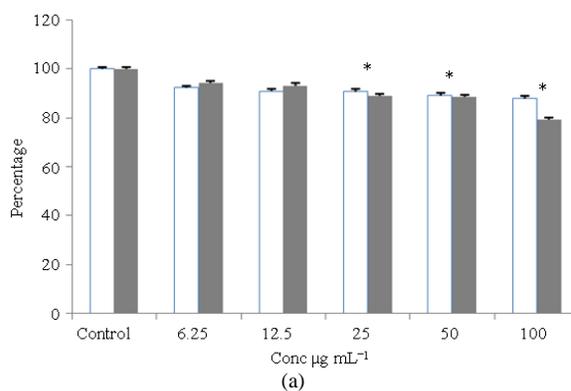


Fig. 4: Cell viability of (a) macrophage cells, (b) hepatocytes, after exposure to SPIONs assayed by MTT (n = 8) after 24 h (blank columns) and 72 h (grey columns) * p<0.001 analyzed by one-way ANOVA versus control groups

After 72 h exposure, however, the decrease was significant at a dose of higher than 25 μg mL⁻¹ (p<0.001), indicating a dose-dependent cytotoxicity of the SPIONs for macrophage cells. Thus, the macrophage cells and hepatocytes responded differently to the SPIONs. The presence of specific protein binding to iron of liver cells while macrophage cells uptake foreign particles via phagocytosis (Shubayev *et al.*, 2009) might be the explanation of the different responses found in this study.

Iron oxide is a metal oxide which can oxidize certain cellular macromolecules including lipids, so TBARS was used to test this hypothesis after cellular exposure to SPIONs. Lipid peroxidation, a major indicator of oxidative stress and measured as TBARS, shown in Fig. 5, is dependent on the type of cells. With macrophage cells, Fig. 5a, a significant increase of TBARS was observed at 100 μg mL⁻¹ (p<0.05) after 24 h; on the contrary, after 72 h at the same dose a decrease was observed, suggesting that cell adaptation occurred as a self-defense antioxidant

response to oxidative stress. For normal liver cells, after 24 or 72 h of exposure to the SPIONs, no significantly change in lipid peroxidation was found (Fig. 5b). This study has further emphasized the effects of cell type, exposure duration and the nature of cell adaptations to the cytotoxicity.

Pro-inflammatory response was investigated using SPIONs as this was found with nanosized TiO₂ and carbon black (Bhattacharya *et al.*, 2009). Nitric oxide (NO) was measured as a signaling molecule vital to pathogenesis due to inflammation and usually overproduced in abnormal physiological conditions (Sharma *et al.*, 1996). As a short-lived highly reactive and rapid diffusible molecule, its targets are numerous including iron clusters. Macrophage cells showed an increase in lipid peroxide susceptible to this effect. However, 24 and 72 h exposure to macrophage cells, SPIONs, up to 100 µg mL⁻¹ did not significantly affect nitric oxide levels (Fig. 6) when compared to the control.

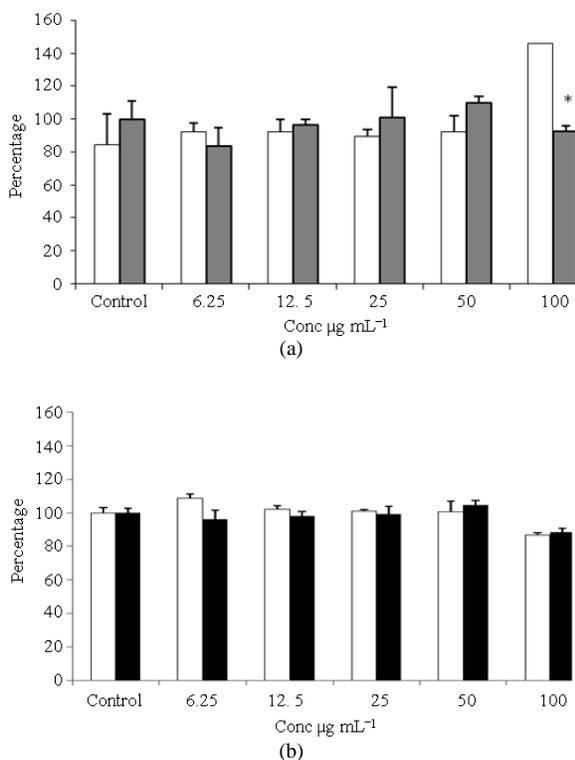


Fig. 5: Lipid peroxidation analyzed by cellular TBARS levels in (a) macrophage cells and (b) Chang liver cells after exposure to SPIONs for 24 h (blank columns) and 72 h (grey columns) (n = 4-6). * p < 0.05 analyzed by one-way ANOVA versus control groups

Figure 7 illustrates microscopic changes of Chang liver cells exposed to various concentrations of SPIONs compared to a negative control. The result confirms that the SPIONs affect cells in a concentration dependent manner and at concentrations of higher than 25 µg mL⁻¹, cell deformation is observed.

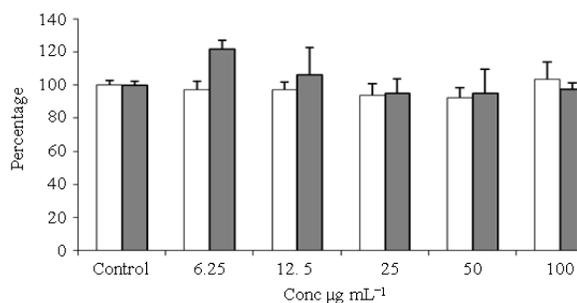


Fig. 6: Effects of SPIONs on nitric oxide level of macrophage cells after exposure for 24 h (blank columns) and 72 h (grey columns), analyzed using Griess reagent and reading the absorbance at 550 nm (n = 6)

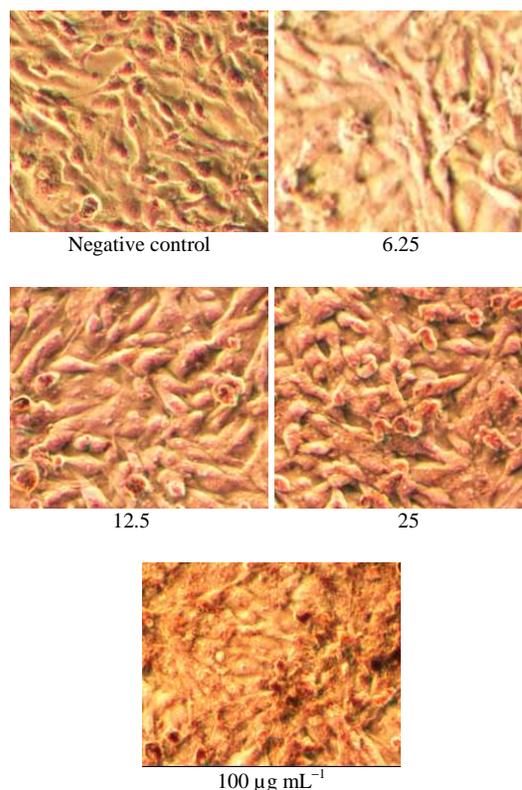


Fig. 7: Microscopic photographs of Chang liver cells exposed to SPIONs at various concentrations for 24 h (×100)

DISCUSSION

The results from XRD and FTIR patterns suggest that the black precipitates obtained from our process are iron oxide of Fe_3O_4 or magnetite. The magnetite produced by this procedure shortens the NMR spin-spin relaxation time (T_2) of protons (^1H) of water containing the particles. Estimation of the relaxation rate, by equation (2), gave $1/T_2^*$ of the SPIONs at 12.5, 25, 50 and 100 g mL^{-1} of 22.6, 60.6, 136.6 and 279.0 sec^{-1} , respectively. Thus, an increase of the concentration of the particles also positively and linearly correlates with the relaxation rate ($r = 0.9987$). This indicates that the particles produced are SPIONs.

It has been shown that the size, shape and composition of nano-particle product depends on the type of salts used, the ratio of Fe^{2+} to Fe^{3+} , pH and ionic strength of the media (Shubayev *et al.*, 2009). A review (Gupta and Gupta, 2005) also suggests that the co-precipitation method used to produce SPIONs requires a non-oxidizing anaerobic environment while Fe^{2+} reacts with Fe^{3+} at a molar ratio of 1:2 and the black precipitates are to be expected at pH 9-14. However, the process used in this study was different. The reaction was simple with an equivalent ratio of about 1:1 with aeration and a neutral pH. The result of this simplified method has proven to be superparamagnetic iron oxide nanoparticles with saturation magnetization of 67.7 emu g^{-1} and coercivity of 34.5 G by vibrating sample magnetometer.

The macrophage cells and hepatocytes responded differently to the SPIONs. The presence of specific proteins binding to the iron of liver cells, while macrophage cells take up foreign particles via phagocytosis (Shubayev *et al.*, 2009), might be the explanation for the different responses found in this study. Previous reports have shown cellular oxidative stress by increased TBARS after exposure to nanoparticles such as SiO_2 and fullerene C_{60} . Using HEK293 cells, lipid peroxidation of SiO_2 nanoparticles has been shown to be size-dependent (Wang *et al.*, 2009). Fullerene C_{60} significantly elevated lipid peroxidation and induced oxidative stress in a fish model (Oberdorster *et al.*, 2006). This study has demonstrated that oxidative induction of nanoparticulates is concerned not only with cell type, but also the exposure duration and the nature of cell adaptations.

Results obtained from our current *in vitro* cytotoxicity study may not be a substitute for studies *in vivo* and that occur throughout the whole body. However, they give a basis for further assessing the potential risk of chemical /material exposure. As far as

the assessment of toxicological properties of nanoparticles is concerned, it is not known how they behave when they are dispersed in exposure media. The method used in the preparation of the SPIONs in this study was shown to be simpler than the previous reports (Lee *et al.*, 2008; Thorek *et al.*, 2006; Teja and Koh, 2009; Verges *et al.*, 2008), however some of the nanoparticles may rapidly agglomerate or settle and need constant stirring to make a homogeneous suspension, and so the full cellular dose/time of these materials would be larger. The other issue that is still not known is whether the cells internalize nanoparticles and if so, what are the mechanisms involved. Iron oxide as a metal oxide could oxidize certain cellular macromolecules including lipids, so TBARS was appropriate for measurement of this effect after cellular exposure to SPIONs. Our results from MTT assay, TBARS assay and NO measurement studies show that nanoparticles are associated with cytotoxicity, oxidative stress and lipid peroxidation formation but normal liver cells did not generate lipid peroxidation when exposed to $\leq 100 \text{ }\mu\text{g}\cdot\text{mL}^{-1}$ of SPIONs. Cell adaptation was also observed as a self-defense antioxidant response to oxidative stress.

CONCLUSION

SPIONs were successfully prepared by a co-precipitation process with pH control at 7 and the optimum equivalent ratio of $\text{Fe}^{3+}:\text{Fe}^{2+}$ was 1:1. Materials which result in cell viabilities higher than 80% are often recognized as biocompatible, thus from the MTT assays conducted here, SPIONs produced by this method can be considered biocompatible, although they cause some cytotoxicity to both the cell types tested here at high concentrations. Furthermore, iron oxide nanoparticles did not induce oxidative stress and lipid peroxidation formation in Chang liver cells. Also, in macrophage cells at high initial concentration up to $100 \text{ }\mu\text{g mL}^{-1}$, using TBARS assay and nitric oxide measurement, SPIONs did not induce the release products of pro-inflammatory response from macrophage cells. However, the toxicity of iron oxide nanoparticles should be further investigated with other cells and other methods.

ACKNOWLEDGEMENT

The researchers would like to acknowledge the financial support of the National Research Council of Thailand (Grant no. PorKor/2552-84). Ms Nittaya Luenam, Ms Narissara Kulanaris and Ms Parichat Phothisai are thanked for their technical assistance.

REFERENCES

- Banaclocha, M.A.M., I. Bokkon and H.M. Banaclocha, 2010. Long-term memory in brain magnetite. *Med. Hypotheses*, 74: 254-257. DOI: 10.1016/j.mehy.2009.09.024
- Bhaskar, S., F. Tian, T. Stoeger, W. Kreyling and J.M. de la Fuente *et al.*, 2010. Multifunctional nanocarriers for diagnostics, drug delivery and targeted treatment across blood-brain barrier: Perspectives on tracking and neuroimaging. *Part. Fibre Toxicol.*, 7: 1-3. DOI: 10.1186/1743-8977-7-3
- Bhattacharya, K., M. Davoren, J. Boertz, R.P.E. Schins, E. Hoffmann and E. Dopp, 2009. Titanium dioxide nanoparticles induce oxidative stress and DNA-adduct formation but not DNA-breakage in human lung cells. *Part. Fiber Toxicol.*, 6: 17. DOI: 10.1186/1743-8977-6-17
- Farrar, T.C. and E.D. Becker, 1971. *Pulse and Fourier Transform NMR: Introduction to Theory and Methods*. 1st Edn., Academic Press, New York, ISBN-10: 0122496507, pp: 118.
- Gupta, A.K. and M. Gupta, 2005. Synthesis and surface engineering of iron oxide nanoparticles for biomedical applications. *Biomaterials*, 26: 3995-4021. PMID: 15626447
- Jones, C.F. and D.W. Grainger, 2009. *In vitro* assessments of nanomaterial toxicity. *Adv. Drug Deliv. Rev.*, 61: 438-456. DOI: 10.1016/j.addr.2009.03.005
- Lee, Y.T., K. Woo and K. Choi, 2008. Preparation of water-dispersible and biocompatible iron oxide nanoparticles for MRI agent. *IEEE T. Nanotechnol.*, 7: 111-114. DOI: 10.1109/TNANO.2007.909949
- Ma, M., Y. Zhang, W. Yu, H. Shen, H. Zhang and N. Gu, 2003. Preparation and characterization of magnetic nanoparticles coated by amino silane. *Colloid Surf. A.*, 212: 219-226. DOI: 10.1016/S0927-7757(02)00305-9
- Marques, R.F.C., C. Garcia, P. Lecante, S.J.L. Ribeiro and L. Noe *et al.*, 2008. Electro-precipitation of Fe₃O₄ nanoparticles in ethanol. *J. Magn. Magn. Mater.*, 320: 2311-2315. DOI: 10.1016/j.jmmm.2008.04.165
- Molday, R.S., 1984. Magnetic iron-dextran microspheres. United States Patent 4452773, June 5. <http://www.freepatentsonline.com/4452773.pdf>
- Oberdorster, E., S. Zhu, T.M. Blickley, P. McClellan-Green and M.L. Haasch, 2006. Ecotoxicology of carbon-based engineered nanoparticles: Effects of fullerene (C₆₀) on aquatic organisms. *Carbon*, 44: 1112-1120. DOI: 10.1016/j.carbon.2005.11.008
- Ohkawa, H., N. Ohishi and K. Yagi, 1979. Assay for lipid peroxides in animal tissues by thiobarbituric acid reaction. *Anal. Biochem.*, 95: 351-358. PMID: 36810
- Pankhurst, Q.A., J. Connolly, S.K. Jones and J. Dobson, 2003. Applications of magnetic nanoparticles in biomedicine. *J. Phys. D Appl. Phys.*, 36: R167-R181. http://www.physics.gla.ac.uk/~dtngo/Article/JPD_36_2003_R167.pdf
- Papell, S.S., 1965. Low viscosity magnetic fluid obtained by the colloidal suspension of magnetic particles. United States Patent 3215572, November 2. <http://www.freepatentsonline.com/3215572.pdf>
- Pei, W., H. Kumada, T. Natusme, H. Saito and S. Ishio, 2007. Study on magnetite nanoparticles synthesized by chemical method. *J. Magn. Magn. Mater.*, 310: 2375-2377. DOI: 10.1016/j.jmmm.2006.10.837
- Sharma, H.S., J. Westman, Y. Olsson and P. Alm, 1996. Involvement of nitric oxide in acute spinal cord injury: An immunocytochemical study using light and electron microscopy in the rat. *Neurosci. Res.*, 24: 373-384. DOI: 10.1016/0168-0102(95)01015-7
- Shubayev, V.I., T.R. Pisanic and S. Jin, 2009. Magnetic nanoparticles for theragnostics. *Adv. Drug Deliv. Rev.*, 61: 467-477. DOI: 10.1016/j.addr.2009.03.007
- Sun, C., J. Lee and M. Zhang, 2008. Magnetic nanoparticles in NMR imaging and drug delivery. *Adv. Drug Deliv. Rev.*, 60: 1252-1265. DOI: 10.1016/j.addr.2008.03.018
- Sun, S. and H. Zeng, 2002. Size-controlled synthesis of magnetite nanoparticles. *J. Am. Chem. Soc.*, 124: 8204-8205. DOI: 10.1021/ja026501x
- Teja, A.S. and P.Y. Koh, 2009. Synthesis, properties and applications of magnetic iron oxide nanoparticles. *Prog. Cryst. Growth Ch.*, 55: 22-45. DOI: 10.1016/j.pcrysgrow.2008.08.003
- Thorek, D.L., A.K. Chen, J. Czypryna and A. Tsourkas, 2006. Superparamagnetic iron oxide nanoparticle probes for molecular imaging. *Ann. Biomed. Eng.*, 34: 23-38. PMID: 16496086
- Verges, M.A., R. Costo, A.G. Roca, J.F. Marco and G.F. Goya *et al.*, 2008. Uniform and water stable magnetite nanoparticles with diameters around the monodomain-multidomain limit. *J. Phys. D Appl. Phys.*, 41: 134003. DOI: 10.1088/0022-3727/41/13/134003

- Wang, F., F. Gao, M. Lan, H. Yuan, Y. Huang and J. Liu, 2009. Oxidative stress contributes to silica nanoparticle-induced cytotoxicity in human embryonic kidney cells. *Toxicol. In Vitro*, 23: 808-815. DOI: 10.1016/j.tiv.2009.04.009
- Wang, J., J. Sun, Q. Sun and Q. Chen, 2003. One-step hydrothermal process to prepare highly crystalline Fe₃O₄ nanoparticles with improved magnetic properties. *Mater. Res. Bull.*, 38: 1113-1118. DOI: 10.1016/S0025-5408(03)00129-6
- Wang, X., C. Zhang, X. Wang and H. Gu, 2007. The study on magnetite particles coated with bilayer surfactants. *Appl. Surf. Sci.*, 253: 7516-7521. DOI: 10.1016/j.apsusc.2007.03.053
- Xu, C. and A.S. Teja, 2008. Continuous hydrothermal synthesis of iron oxide and PVA-protected iron oxide nanoparticles. *J. Supercrit. Fluid.*, 44: 85-91. DOI: 10.1016/j.supflu.2007.09.033